

# *Image Enhancement of Metastasis And Acrometastasis Images Using Clahe With Weiner Filter*

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**Abstract** - Bony metastases arise in 30% of all cancers, but only 1% to 3% of these developments in the side. The lung is the most common micrometastasis site, accompanied by breast and renal cell disease. The use of automated systems in clinical imaging evaluation has shown to be quite helpful to cardiologists, especially in research schemes where radiologists make their actual diagnosis on the basis of observations only, many of them apply to healthy individuals and at the initial stage have to differentiate between harmful and non-pathological findings. Artifacts and variability influence the consistency of the study in intensity. We, therefore, need an optimized methodology of rectification to remove the objects and the difference in intensity current in the picture. Methods of preprocessing make the sample suitable for more production. It improves the image's value and ultimately eliminates the noise in the film. Preprocessing methods aim to improve the picture while modifying the quality of the data. In this paper, before discussing lung cancer diagnosis, we suggested the most important and necessary preprocessing approaches for metastasis and micrometastasis designs. Initially, the RGB picture is transformed into the Image grayscale to perform adaptive histogram equalization (CLAHE) that restricted to contrast. Therefore the elimination of noise is done with a Wiener filter. The median filter is used in the existing system for eliminating unnecessary objects. The efficiency of the proposed preprocessing method is then related to current technology.

**Keywords** - *Acrometastasis, CLAHE, lung cancer, metastasis, noise removal, preprocessing, wiener filter.*

## I. INTRODUCTION

Image preprocessing is the first and essential technique involved in lung cancer detection. The preprocessing method is needed to improve the detection accuracy and to eliminate some regions of

CT Image such as background and surrounding tissues or vessels. Metastasis happens more often through the bloodstream or lymph process. Cancer cells must have a blood supply to work just like healthy cells. Like healthy cells, they have links to the bloodstream. Such a connection enables the typical circulation of the bodies to join removed malignant cells from the tumor. The cancer cells now have spread to all parts of the body once in the blood. Like the circulatory system, the lymph scheme has its pathways across the organization, through which a malignant cell can pass. Once surgeons remove a tumor, they may also eliminate surrounding parts of the lymph system, such as the lymph nodes, since these are often the first sites of metastasis of the cancers. When metastasis has happened to the lymph system, the cure prognosis decreases considerably.

Acrometastasis is a rare occurrence in the face. The distal phalanges are the most common site of metastatic accumulation, while it has been identified as participating in all bones of the hand. Metastasis frequency in metacarpals is 17%, phalanges 66%, and carpal bones 17%. The lung is the most popular source, with breast and kidney accompanied by 42 percent, each accounting for 11 percent. Specific causes involve cancers of the colon, prostate, thyroid, esophagus, and bone. [1]. Metastases typically involve the skeletal structures of the hand, although soft tissue lesions can occur as a result of tumor erosion or direct seeding. The mechanism by which tumors metastasize to the side remains obscure. A variety of factors, including

trauma, thermal tissue differences, hormonal influence, hemodynamics, and host immune responses, have all been implicated.

[2] Hematogenous dissemination of tumor emboli is the presumed mechanism in the majority of cases. Within areas affluent within red marrow, bone metastases usually develop. The small amount of this tissue in the bones of the hand supports findings in the literature, which indicate that secondary lesions in the end regions of the extremities are quite remarkable. The patient's side is usually painful, swollen, erythematous, and wet. The x-rays show damage to the lytic bone. The differential diagnosis involves gout, infection with pulp, osteomyelitis, septic arthritis, rheumatoid arthritis, tenosynovitis, and sympathetic dystrophy with reflex.

A malignant cell must first break away from the cancer tumor to begin the cycle of metastasis. Cells bind to each other in healthy tissue, as well as a web of protein that fills the space between them. This web of protein is called the extracellular matrix. Typical of the epithelium, the cell levels that make up the edges and mouth, abdomen, lungs, and other bodies is this connection between the cells and the extracellular matrix.

Acrometastasis is rare and mimics an infectious or inflammatory disorder in its appearance. Therefore, this detection is often delayed, especially in cases where there is no suspicion of primary cancer. In the hand of an untreated non-small cell lung cancer, our sufferer had metastasis and demonstrated that micro metastasis had to be included in coefficient.

## II. RELATED WORK

JIE WEI et al. [3] introduces concepts and techniques through image / signal processing, big data and machine learning to 4DCT lung data to fully automatic lung division, lung characteristics can be visualized and analyzed on fly by user experiences, and categories of data capture can be robustly defined. Comparisons of our results with an established treatment planning system and expert assessment revealed small differences (within  $\pm 2$  percent) but quality-enhancing one to two magnitudes. A Fourier analysis-based analytical value

evaluation performance closely emulates human expertise.

Nidhi S. Nadkarni et al. [4] in CT scanning photos, provide an automatic strategy for detecting lung cancer. The lung cancer detection method suggested using strategies such as median filtering for preprocessing images accompanied by optimization of the lung region of interest using morphological mathematical operations. Geometric characteristics are determined from the derived section of the value and are used to identify CT scans into normal and abnormal by using a vector supporting computer.

Desiree Juby Vincent et al. [5] summarizes the design of a changed non-linear anisotropic diffusion filter where local noise estimates are estimated on the basis of the mean square error. Also, unsharp masking is used to improve the edge. Based on the finite-difference principle, this filter is applied. Experimental results on CT photos indicate that noise is limited due to the objects, and advantages are well maintained. If the brightness gradient created by the sound is lower than the margins, conventional diffusion filters perform better.

Gilberto de Melo et al. [6] presentation of the automated system has high computing costs. This paper introduces an explicitly constructed CUDA-based parallel method to deliver performance gains for a wavelet drilling function added to high-resolution DICOM pictures. To classify pneumonia, the wavelet characteristics are used, as well as the proposed parallel approach improves the processing rate by more than 12.75 fold.

Agus Maman Abadi et al. [7] proposes the improvement of chest x-ray images with until checking them for a fair or lung cancer classification, high-frequency concentration filter and histogram equalization. The study is conducted using the RBFNN algorithm with the characteristics obtained by the GLCM method from the chest x-ray images. In order to generate the RBFNN model, we want unattended and supervised learning techniques to learn the methods of clustering K-means and regional ridge reconstruction.

Shih-Che Chien et al. [8] introduces an important hybrid approach to improving contrast images that

combine local information and global data. It thus offers an enhanced environmental effect in regional areas without creating visual objects or halo. Findings show that our method produces enhanced visual quality images that are higher than the GHE process.

Avinash S et al. [9] a new method is introduced with Gabor Filters, Discrete Wavelet Transform, and Auto Enhancement Algorithm to address image improvement disadvantages. Using various techniques — in this study, Gabor filter, DWT, and AEA-X-ray lung images are viewed and evaluated. The results obtained are comparable with typical results for real-time evaluation. Using the Gabor filter for image enhancement, a new method can be used to quickly identify cancer cells in patients.

Kai-Lung Hua et al. [10] introduces a practical approach for improving image contrast, mixing local and global knowledge. In disaster recovery, the method of reciprocal mean-separate histogram equalization gives us multiple intensity mapping features. We map different conversion features according to the intensity level to the sub-block core and its neighboring sub-blocks. In order to improve the local clarity of the image, this process is correlated with unsharp erasing.

Fan Xu et al. [11] proposes a new enhancement filter for the identification nodules in the regions of the lungs. Using the pixel consistency features and the nodule sector form attributes, the proposed screen will enhance nodule-like components and limit line-like regions and edge regions. The Integral Image Technique (IIT) is also used to increase the processing speed of the filter.

Avinash. S et al. [12] use Gabor filters and watershed segmentation methods to introduce a new process of detecting lung cancer. The CT (Computed Tomography) images taken from patients with lung cancer are evaluated by designing a handling strategy for digital photos. The findings obtained for real-time evaluation are equivalent to the regular results collected from the hospital. Therefore, the new method can be used to quickly identify lung cancer with Gabor filters and a procedure of watershed optimization.

Sruthi Ignatius et al. [13] in general, Computed Tomography (CT) images are used for cancer diagnosis. The different phases of computer-aided pulmonary cancer diagnosis are development, segmentation, and collection of features. There are several methods for these levels to be performed. Such various methods have been described in detail.

### III. PROPOSED METHOD

The input picture may have noise and unnecessary signals that occurred during the patient's movement or image creation. The preprocessing measures of the image include the reduction of noise. The picture equalization method is performed to enhance the quality of the picture. In preprocessing, we smooth and sharpen the image by the sticks without losing its main characteristics of diagnostic objects. To obtain picture highlights, we use various filter strategies such as median and Wiener filters. To reduce the impact of unwanted noise, we use the Wiener filter. Wiener filter is favored as it has the lowest noise-related peak signal. Wiener filter is mainly used in the development of digital images. It is often used by linear invariant methodology in the de-convolution method to reduce noise. This tests the stationary signal, spectrum of sound, and noise additives. Such artifacts are identified and eliminated. Wiener filter also lowers the Mean Square Error (MSE) between the estimated and desired blur signals of the image.

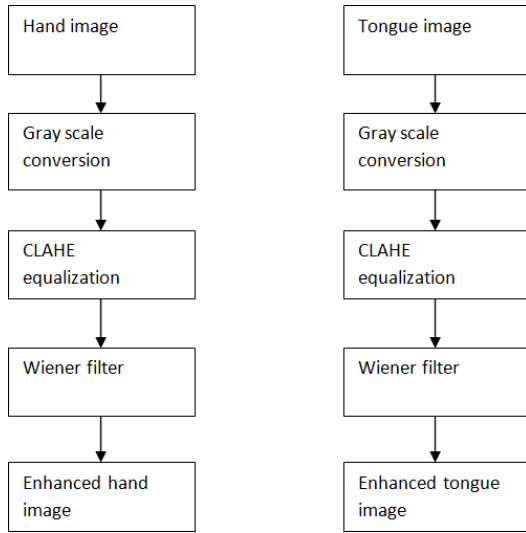


Fig. 1. Block diagram of the proposed method

It is a challenging task to process a picture. It is essential to remove unnecessary items that it can carry before any movie can be handled. The image can be analyzed effectively after removing unnecessary artifacts. Image Preprocessing is the first step in the production of images. This is used to improve the likelihood of finding the area concerned. Preprocessing requires procedures such as converting the image to gray, removing noise, and reconstructing images. The most common preprocessing practice is the transformation to grayscale Image[14]. Using specific filtering approaches to remove excess noise after the image is transformed into grayscale.

Preprocessing requires procedures such as gray image transformation, noise reduction, and picture restoration. The most normal practice in preprocessing is the transformation to a grayscale image. Once the painting is transformed into grayscale, using various filtering approaches to remove excess noise.

#### A. Equalization of Restricted Adaptive Histograms

CLAHE was a lot than AHE. CLAHE algorithm breaks the image into tiles, i.e. background regions. It generates the graph of each contextual field, and the clipping takes place at a predetermined value. The

clamped quantity is shared among the histogram bins. This vectorscope is the altered form of the original histogram. This strategy solves the rim-shadowing effect of AHE and eliminates the problem of over-enhancing. CLAHE has shown its effectiveness in improving medical images with low contrast. The parameters to be considered for CLAHE are the histogram clip cap and background area scale. Such parameters can affect the efficiency of the CLAHE. This method makes the secret characteristics of the picture more apparent by redistributing the used gray value. Various transformations can be computed using the CLACHE algorithm assuming the value of the frequency. Consider an image 'Q' of  $N \times N$  pixel of range P (i, j). The image 'Q' produces an image 'R' of the same  $N \times N$  pixel. Then the equation is given by

$$P_n = 255 \left( \frac{|\varphi_w(P) - \varphi_w(\min)|}{|\varphi(\max) - \varphi_w(\min)|} \right) \quad (1)$$

$$\varphi_w(P) = \left[ 1 + \exp\left(\frac{\mu_w - P}{\sigma_w}\right) \right]^{-1} \quad (2)$$

#### B. Wiener Filter

A kernel's convolution with the image pixels, defined by a Gaussian function. In the discrete case, the convolution is given by

$$f * g[n] \stackrel{\text{def}}{=} \sum_{m=-\infty}^{\infty} f[m] \cdot g[n - m] \quad (3)$$

The two-dimensional Gaussian function is the function used to produce the kernel. In the following purpose, A is the amplitude,  $(x_0, y_0)$  the center,  $\sigma_x, \sigma_y$  the standard deviations in the x and y directions. The kernel size is 3x3.

$$f(x, y) = A \cdot e^{-\left(\frac{(x-x_0)^2}{2\sigma_x^2} + \frac{(y-y_0)^2}{2\sigma_y^2}\right)} \quad (4)$$

Due to its simplicity and speed, the Wiener filter is commonly used. It is considered pure as it uses a linear equation system to measure a set of optimum filter weights that lowers a received signal's noise level. To calculate these weights, it calculates bend-correlation and covariance matrices of noisy signals and provides a precise estimation of unmistakable probabilistic signal under linear noise. The noise

numbers are computed and used to assess the filter's optimum weight. By analyzing a new input signal with identical noise traits with optimal filtration weights, the probabilistic message parameter is derived. This method is optimal if the noise distribution is Gaussian. Furthermore, the implementation-only requires a few formal steps that can be completed very easily.

### C. Wiener Filter in the Fourier Domain

$$(u, v) = \left( \frac{H^*(u, v) P_s(u, v)}{|H(u, v)|^2 + P_n(u, v)} \right) \quad (5)$$

$$G(u, v) = \left( \frac{H^*(u, v)}{|H(u, v)|^2 + \frac{P_n(u, v)}{P_s(u, v)}} \right) \quad (6)$$

$(u, v)$  – The role of degradation

$H^*(u, v)$

– Complex decomposition function conjugate

$P_n(u, v)$  – Noise Spectral Energy Density

$P_s(u, v)$

– Power Celestial Undegraded Image Density

The Wiener filter is being used to extract the noise from a detected distorted image based on statistics obtained from a local neighborhood of each pixel. This filter depends on the power of the noise. When the variation is big, the filter smoothed little and the filter smoothed more when the variance becomes small. [15]

#### Algorithm 1: Proposed Algorithm

Input: Image

Output: Enhanced Image

1. Read an image
2. Convert the image into a grayscale image
3. Apply CLAHE equalization by using equation (1)
4. Calculate Gaussian kernel using equation (4)
5. Perform wiener filter using equations (5) and (6)
6. Obtain Enhanced Image

### D. Median Filter

It is one of the most frequently used noise reduction approaches. This is a nonlinear filtering method. Its median filter is based on the normal distribution of the pixel. The benefits of the median filter are that it is sufficient to reduce salt and pepper and speckle vibration. It also protects

the edges and boundaries. The key disadvantages are difficulty and time usage. The Median filtering implementation algorithm can be represented as follows: A filter mask (5x5) consisting of 8- is used in a neighborhood with the (i, j) middle. Suppose A is the picture input obtained after preprocessing, F is the filter masks moving 5x5, and M is the image throughput. Using Equation 7, pixel values are ordered in ascending order in the 8-neighborhood filter mask. The median is calculated by filtering in ascending order all the benefits of a pixel and replacing the pixel calculated by the pixel's average value. Suppose the image neighboring pixel to

consider is an odd number of pixels, then the intermediate pixel values will be replaced. Hence, the median cost determined by using Equation 8. The amount of  $M_{i,j}$ , is then replaced by the obtained median value. This action is done by using Equation 9.

For every point selected in the neighboring pixel of (5x5) image,

$$A = a_{11} \dots a_{ij} \dots a_{mn} \quad (7)$$

$$\text{where } i = 1, 2, 3 \dots m, j = 1, 2, 3, \dots n, m = n = 3, 5, 7$$

$$\text{orde}(A) = a_{11} < \dots < a_{i-1, j-1} < a_{ij} <$$

$$a_{i+1, j+1} < \dots < a_{mn} \quad (8)$$

$$\text{Hence, } M_{ij} = a_{ij} \quad (9)$$

Where  $M_{ij}$  is the Median.

## IV. RESULTS AND DISCUSSION

Image reprocessing plays an important role in the field of image analysis. In this section, we use the CLAHE & Wiener filter to present experimental data from hand and tongue images. The method proposed is designed to support the identification of lung cancer using photographs of the hand and tongue. The experimental results obtained from the approach proposed are given in Table 1 and Table 2. Table 1 and Table 2 show performance metrics for enhancement techniques after processing. Fig 2 shows the results obtained after the images of the language have been preprocessed. Fig 3 displays the results obtained after hand images have been preprocessed.

### A. Image Quality Measures

It is possible to assign picture quality assessments based on the original image availability. It is necessary to equate the enhanced image with the image. Improved color reproduction was evaluated by various means in this paper. The parameters for assessment are as follows.

*B. Mean to norm ratio of deviation*

Mean-to-standard deviation ratio (MSR) it really is easy to calculate the mean and standard deviations. MSR is the mean-to-standard deviation ratio. It's better for MSR to rise.

*C. Mean Square Error*

MSE is the mean square cumulative error between the original image and the filtered image. For pictures x and y, x has taken to be a unique image while y is assumed to filtered image; hence MSE could be computed using Equation 10.

$$MSE(x, y) = \frac{1}{N} \sum_{i=1}^N (x_i - y_i)^2 \tag{10}$$

*D. Peak signal-to-noise ratio*

The dB (decibels) describes the peak signal-to-noise ratio[20]. PSNR cannot determine image similarity across contrast-enhanced forms. PSNR is defined as

$$PSNR = 10 \log_{10} \frac{R^2}{\sqrt{MSE}} \tag{11}$$

The higher the correct PSNR, the production picture quality. It is the ratio of the signal's maximum power to the power of perverting noise that affects its representation's fidelity. Where R-Maximum input image data type fluctuation. Table 1 displays the output calculation of the MSR, PSNR, and MSE values for the experimented image filtering process.

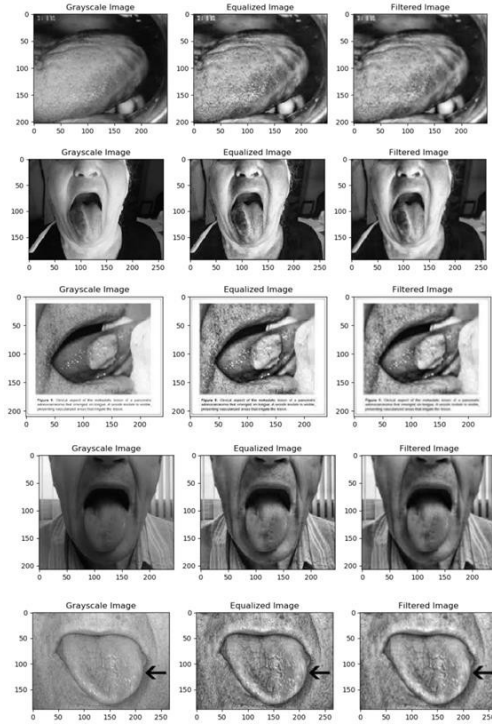


Fig. 2. Experimental data of the language using the approach proposed

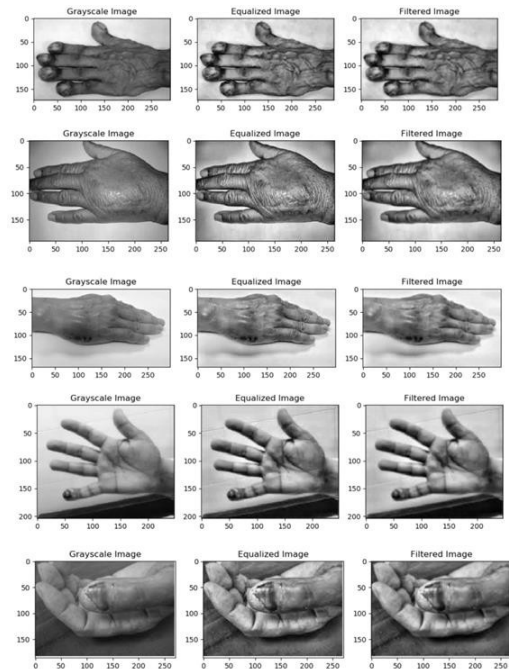


Fig. 3. Experimental hand tests using the process proposed

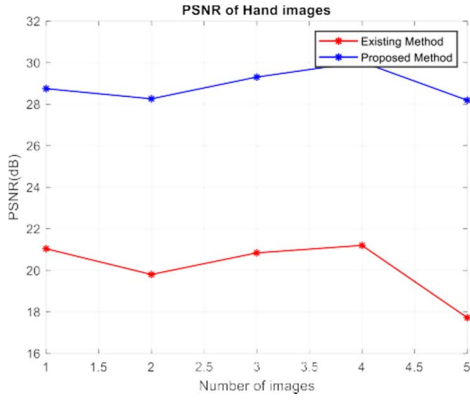


Fig. 4. PSNR analyses of photographs by hand

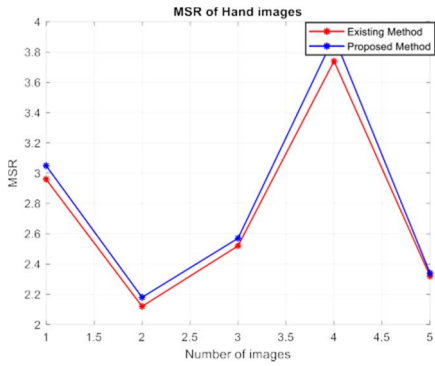


Fig. 5. MSR identification of photographs by hand

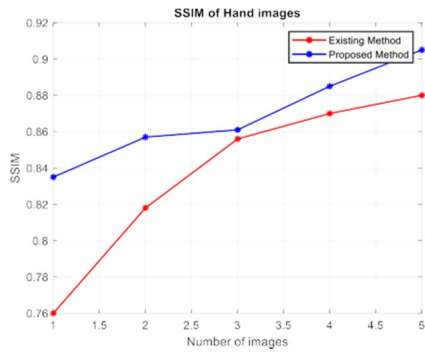


Fig. 6. SSIM hand picture relation

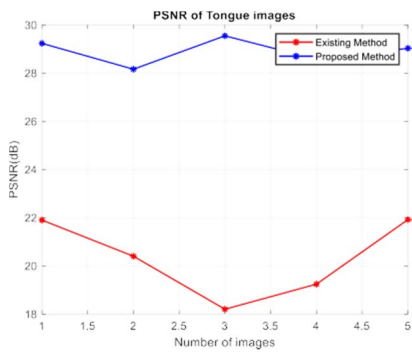


Fig. 7. PSNR contrasts of pictures in the language

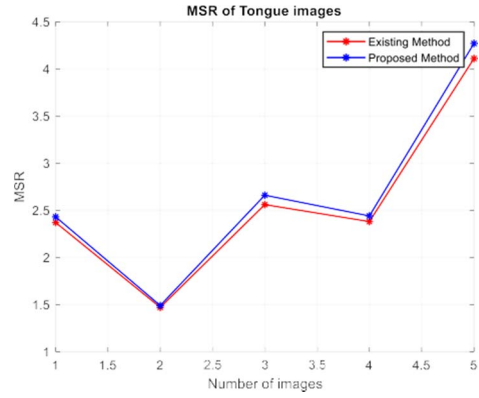


Fig. 8. MSR identification of pictures in the language

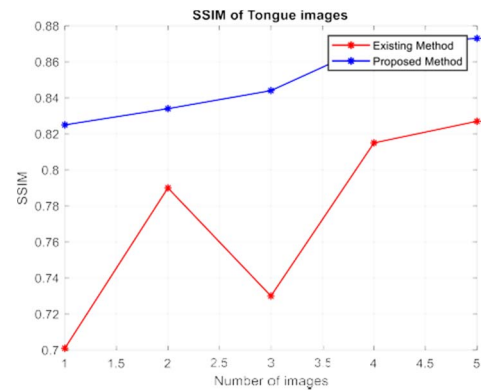


Fig. 9. SSIM identification of pictures in the language

TABLE I.  
COMPARISON OF THE PRESENT AND PROPOSED SYSTEM  
FOR HAND PICTURES

Performance metrics	Existing method (Median filter)	The proposed method (Wiener filter)
MSR	2.7320	2.8080
SSIM	0.8368	0.8686
PSNR	20.1200	28.9066

TABLE II.  
COMPARISON OF THE CURRENT AND PROPOSED  
TONGUE IMAGES PLAN

Performance metrics	Existing method (Median filter)	The proposed method (Wiener filter)
MSR	2.5780	2.6580
SSIM	0.7726	0.8492

PSNR	20.3320	28.9086
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## V. CONCLUSION

Medical objects are often only influenced by noise due to both image retrieval from therapeutic approaches and image delivery from patterns to workspace within the central computer network. It noisy usually affects the quality of the original photos to make the diagnosis more accurate; the reprocessing of images has always been provided in the processing of medical images. In this study, using the Wiener filter, they have put in place a fairly simple and efficient method to eliminate Gaussian noise from medical images. A Wiener filter is a perfect filter when it comes to noise reduction or image de-blurring. When part of the study of a copy, it discusses both the role of degradation and sound. The experimental results show the reliability of the Wiener filter and the protection of data. Thanks to its simplicity and speed, the Wiener filter is widely used. The experimental results indicate that the proposed method's effectiveness.

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